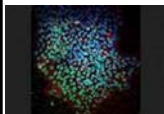
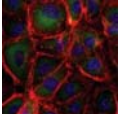


## Regenerative Strategies for Replicating IVD Structure

2016 Castellvi Spine Symposium  
May 19-22



Daniel A. Grande, Ph.D.  
Dept of Orthopedic Surgery  
Feinstein Institute for Medical Research  
Northwell Health System  
Manhasset, NY 10030



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### Disclosures:

- Aedicell, Inc.: Consultant, SAB member
- Histogen, Inc; Consultant
- Regen Labs; Consultant
- Suneris, Inc. Consultant/ Stock option holder

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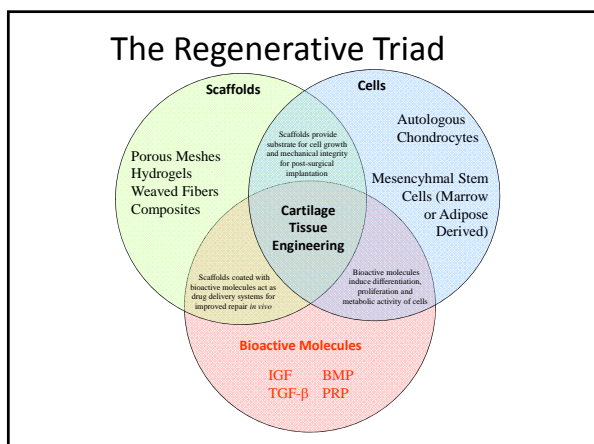
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### Characterization of MSC's

- Non hematopoietic multipotent cells
- High proliferative potential
- Ability to differentiate into:
  - Chondrocytes, osteoblasts, adipocytes, and stromal cells
- Immunomodulatory activity
  - Contribute to immune suppression
  - Tissue healing
- Potential use in tissue regeneration therapies
- Reserve to replace damaged and aged cells

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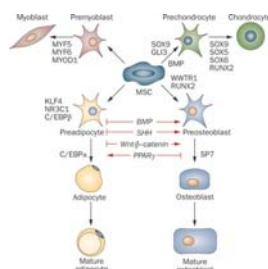
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### multiple differentiation potential

- Major source:
  - Bone marrow derived
  - Adipose derived
- Major applications in orthopaedics:
  - Spine fusion, Vertebral body repair (osteogenesis)
  - Cartilage, Intervertebral disc regeneration (chondrogenesis)



Takeda, I. et al. Wnt and PPARγ signaling in osteoblastogenesis and adipogenesis  
*Nat Rev Rheumatol.* 2009 Aug;5(8):442-7. Epub 2009 Jul 7.

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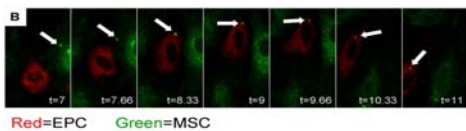
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### Paracrine Stimulation by stem cells

- Coculture of endothelial cells and bone marrow MSC's



A vesicle transported from MSC to endothelial cells. Time is indicated as hours

Aguirre A. et al. Dynamics of bone marrow-derived endothelial progenitor cell/mesenchymal stem cell interaction inco-culture and its implications in angiogenesis.  
*Biochem Biophys Res Commun.* 2010 Sep; 17:400(2):284-91

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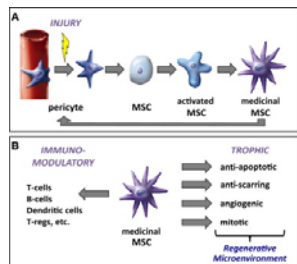
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### Mechanism of Action of MSC's as an Adjunct in Cartilage Repair

'We call MSCs medicinal signalling cells'



Caplan and Correa. Cell Stem Cell 2011;9:11

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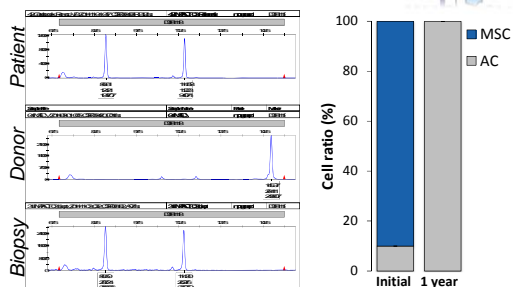
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### MSCs stimulate cartilage repair

impact.



90 % allogeneic MSCs facilitate 100% autologous repair tissue

Vonk, Saris. UMC Utrecht, IMPACT trial

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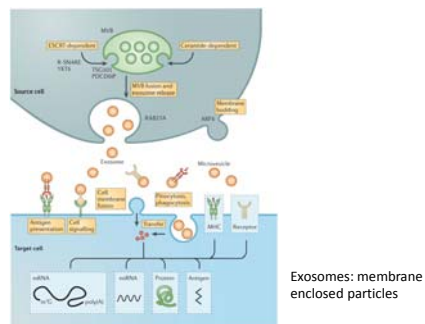
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### Extracellular vesicles - biogenesis



Exosomes: membrane enclosed particles

Andaloussi et al. Nat Rev Drug Discov. 2013;12:347-57

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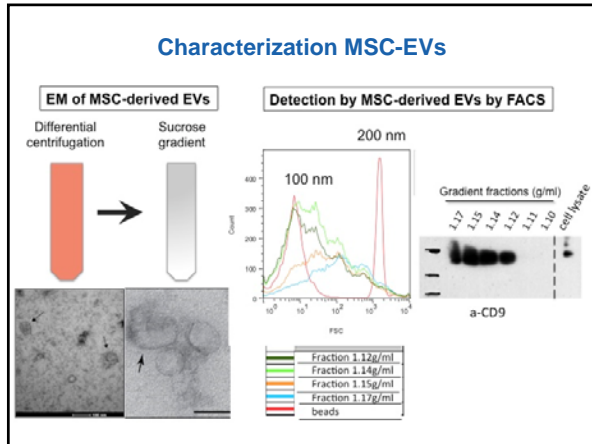
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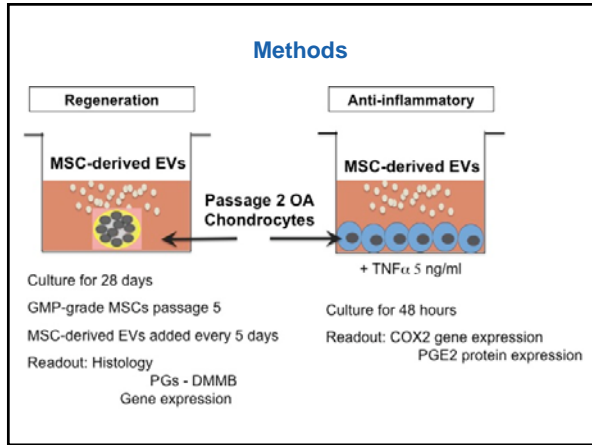
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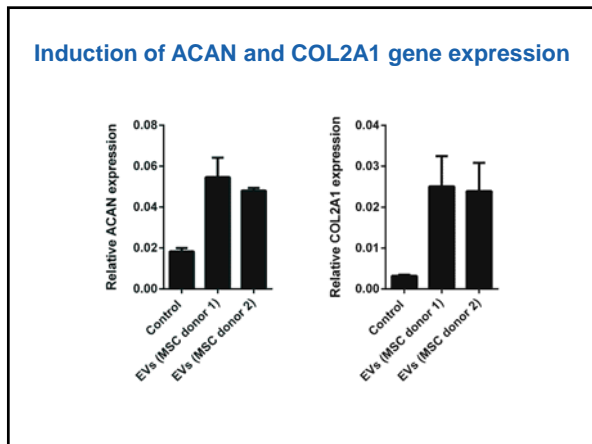
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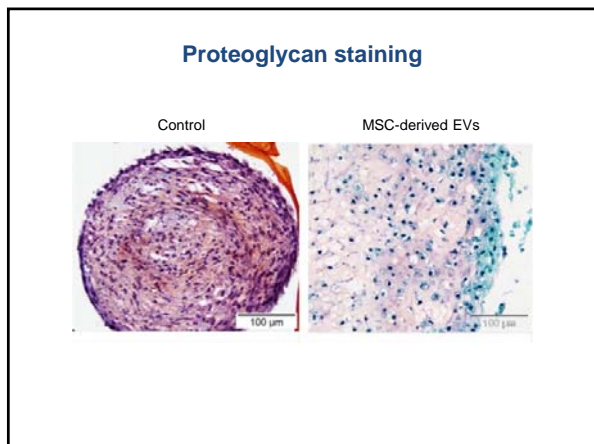
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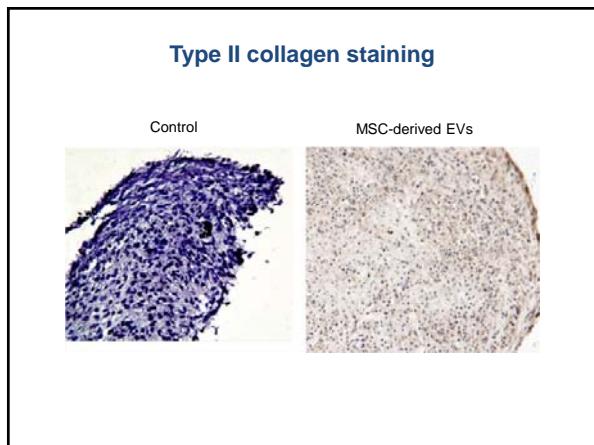
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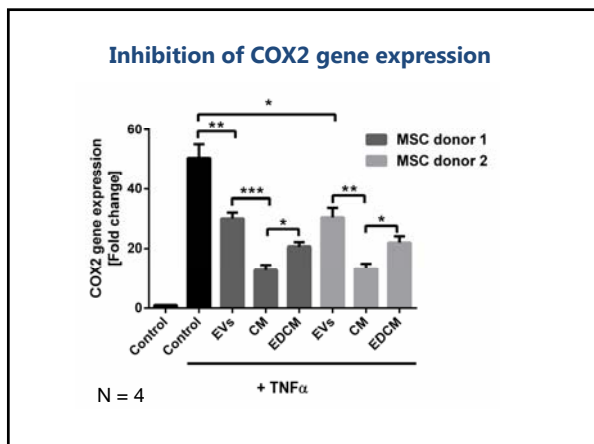
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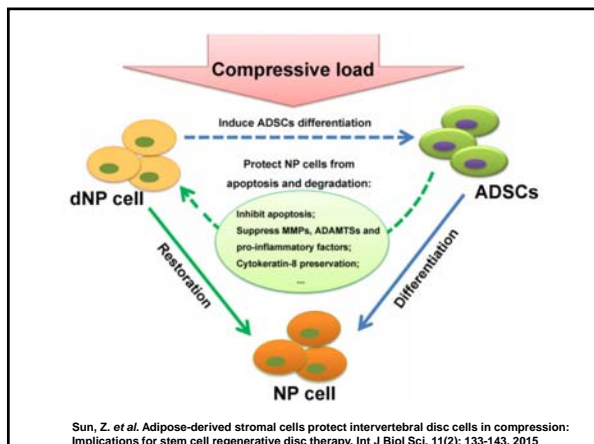
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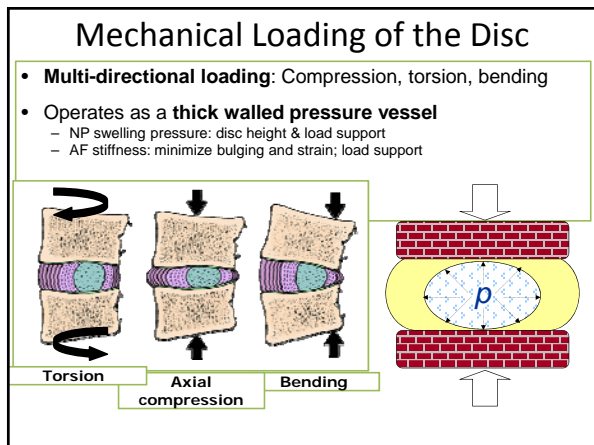
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### Low Back Pain and Disc Degeneration

- Annual societal burden over \$100 billion
- #1 cause of activity limitation in adults < 45 y.o.

Medieval!  
(and they might not work)

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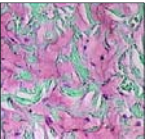
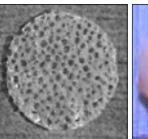


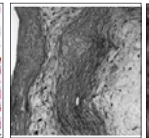
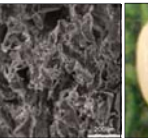

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### Materials for Disc Tissue Engineering

			
<b>Alginite/Chitosan</b> Shao and Hunter, 2007	<b>Collagen/HA</b> Alini et al., 2003	<b>Atellocollagen</b> Sato et al., 2003	<b>PLGA/Alginite</b> Mizuno et al., 2006
			
<b>Gelatin/PCL</b> Wan+, 2008	<b>PCL nanofibers/HA</b> Nesti and Tuan, 2007	<b>Porous Silk</b> Chang et al., 2010	<b>Alginite/Collagen</b> Bowles et al., 2011

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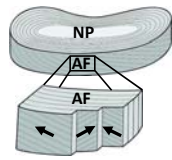
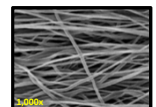
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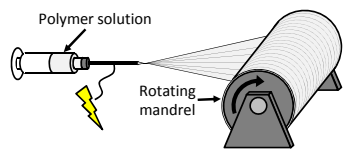
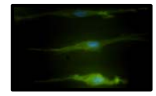
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### Engineered Annulus Fibrosus

- Hierarchical structure:
  - Lamellae: discrete fibrous sheets
  - Fiber alignment: 20° to 50° to the transverse plane (Holzapfel+ 2005)
- Electrospun polymers recreate AF fiber architecture (Nerurkar+ 2007, 2008, 2009, 2010; Driscoll+ 2011)

Nathan+ 2010

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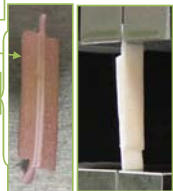
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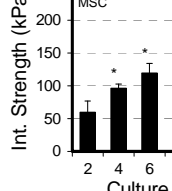
### Multi-Lamellar Nanofibrous Assemblies

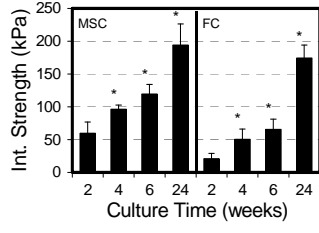
**Conjoined Culture**



Overhang  
Porous Holder  
Interface Region

**Lap Testing**





Culture Time (weeks)	MSC Int. Strength (kPa)	FC Int. Strength (kPa)
2	~60	~20
4	~100*	~50*
6	~130*	~70*
24	~190*	~170*

Mechanically viable interface forms between apposed MSC-laden nanofiber layers

Baker et al., 2007

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### Fabrication of Ordered Bi-Layers

**Goal:** Fabrication of biologic angle-ply laminates to recreate the unique structural hierarchy of the native AF

1. Stack      2. Assemble      3. Culture

Nerurkar et al., 2009

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### Evaluation of Ordered Bi-Layers

- Fabrication of MSC seeded angle-ply biologic laminates
  - Opposing: +/- 30°
  - Parallel: +/- 30°
- Culture in vitro for up to 10 weeks
- Mechanical, biochemical, and histological evaluation

30° opposing      30° parallel

L1      L1

L2      IL

Compositional equivalence between constructs (sGAG, collagen)

Nerurkar et al., 2009

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### Mechanics of Ordered Bi-Layers

- Uniaxial and Biaxial Testing: opposing bi-layers are significantly stiffer than parallel bi-layers (#p<0.05)

Weeks	Parallel (MPa)	Opposing (MPa)
2	~6	~8
4	~7	~10
6	~8	~12
10	~10	~14

Initial      Native

Parallel      Opposing

Nerurkar et al., 2009; Driscoll et al., 2012

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### Rat Caudal Spine Model

- Implantation of Acellular DAPS
  - Little matrix deposition within dense PCL scaffold

Martin+ Acta Biomater 2014

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### I. DAPS Implantations with External Fixation

- DAPS are retained in 100% of surgeries

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### I. DAPS Implantations with External Fixation

- DAPS are retained in 100% of surgeries

	Discectomy	Fixation/ Discectomy	Fixation/ DAPS	Fixation/DAPS (Polarized Light)
Day 14				
Day 28				

Martin+ Acta Biomater 2014

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## Objectives

- I. **Improve retention** of DAPS implanted into the rat caudal spine.
- II. **Improve matrix formation** in implanted DAPS.

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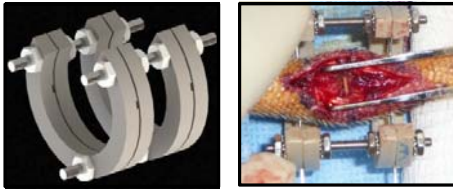
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### I. DAPS Implantations with External Fixation

- Radiolucent ring-type external fixator (Iatridis+ 1999)
- **Implant:** AF-only DAPS, electrospun PCL
- **Procedure:** Insert wires, apply fixator, discectomy, implant
- **Groups:** (n=2-5/group)
  - Fixation+DAPS: 14 days, 28 days
  - Fixation+Discectomy: 14 days, 28 days




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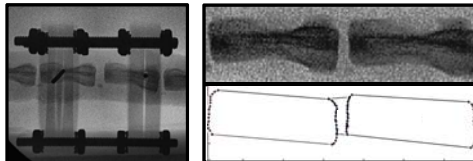
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### I. DAPS Implantations with External Fixation

- Radiolucent ring-type external fixator (Iatridis+ 1999)
- **Implant:** AF-only DAPS, electrospun PCL
- **Procedure:** Insert wires, apply fixator, discectomy, implant
- **Groups:**
  - Fixation+DAPS: 14 days, 28 days
  - Fixation+Discectomy: 14 days, 28 days
- **Analysis:** Fluoroscopy – DHI (Masuda+ 2005),  $\mu$ CT, Histology




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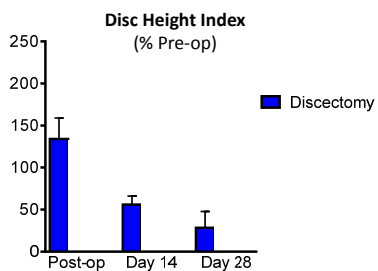
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### I. DAPS Implantations with External Fixation

- Fixation preserves disc height for DAPS and discectomy groups



Martin+ Acta Biomat 2014

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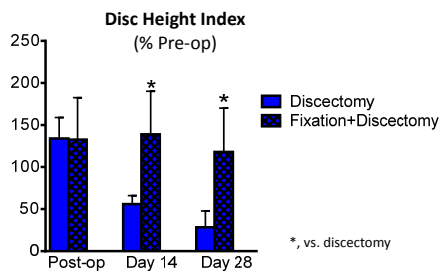
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### I. DAPS Implantations with External Fixation

- Fixation preserves disc height for DAPS and discectomy groups



Martin+ Acta Biomat 2014

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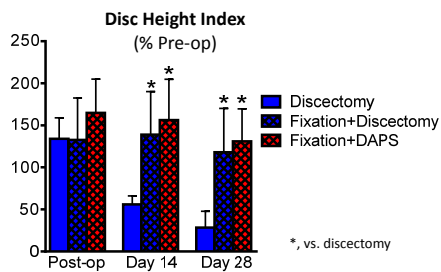
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### I. DAPS Implantations with External Fixation

- Fixation preserves disc height for DAPS and discectomy groups



Martin+ Acta Biomat 2014

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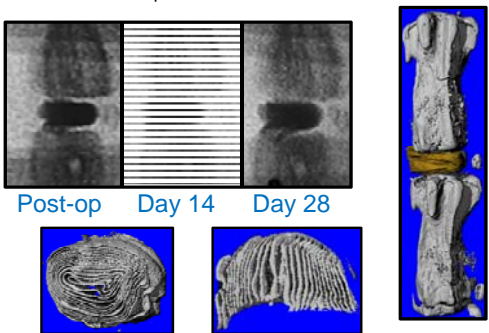
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### I. DAPS Implantations with External Fixation

- rDAPS maintain position with fixation



Martin+ Trans ORS 2014

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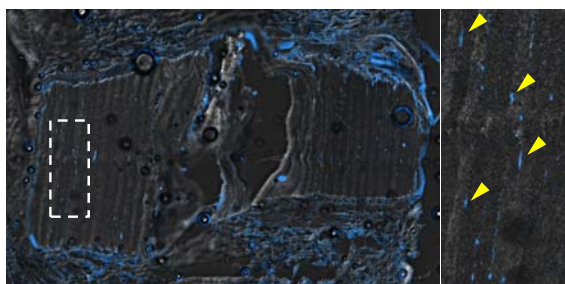
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### I. Development and Validation of Model

- Surgery 2: Implantation of DAPS with External Fixation
  - Sparse cellularity, cells with elongated nuclei



Martin+ Acta Biomater 2014

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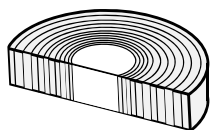
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### II. Sacrificial Layer DAPS (sDAPS)

- Fabrication of sDAPS
  - Water soluble PEO or PLGA layers between PCL layers

PCL



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### II. Sacrificial Layer DAPS (sDAPS)

- Fabrication of sDAPS
  - Water soluble PEO or PLGA layers between PCL layers

PCL PEO

Layer dissolves immediately

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### II. Sacrificial Layer DAPS (sDAPS)

- Fabrication of sDAPS
  - Water soluble PEO or PLGA layers between PCL layers

PCL PEO PLGA

Layer dissolves immediately

Layer dissolves over the course of days

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### II. Sacrificial Layer DAPS (sDAPS)

- In vitro* and *in vivo* evaluation of sDAPS

*In vitro*

wash

seed

seeded cells

*In vivo*

implant

infiltrating cells

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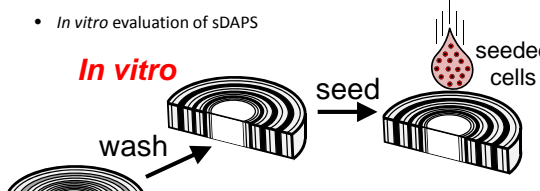
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### II. Sacrificial Layer DAPS (sDAPS)

- In vitro* evaluation of sDAPS



**In vitro**

wash → seed → seeded cells

- ♦ Bovine AF cells, 28 days
- ♦ **Groups:** (n=3/group)
  - DAPS
  - Thin sDAPS – 125 μm PEO
  - Thick sDAPS – 250 μm PEO
- ♦ Analysis: Histology – DAPI

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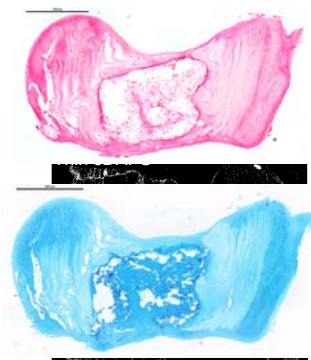
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### II. Sacrificial Layer DAPS (sDAPS)

- In vitro* evaluation of sDAPS
  - PCL-only DAPS were poorly infiltrated
  - AF cells penetrated full height of both thick and thin sDAPS
- Long term culture
  - NP cell seeded Hyaluronic Acid NP region
  - AF cell-seeded AF region
  - 5 and 10 weeks
- Increasing matrix content and mechanics




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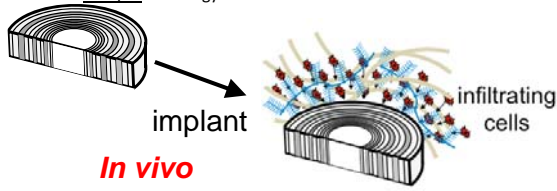
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### II. Sacrificial Layer DAPS (sDAPS)

- In vivo* evaluation of acellular sDAPS
  - Rat caudal disc model
  - **Groups:**
    - PEO sDAPS: thin, 14 days (n=3/group)
    - PLGA sDAPS: thin, 14 days (n=3/group)
  - Analysis: Histology – H&E



**In vivo**

implant → infiltrating cells

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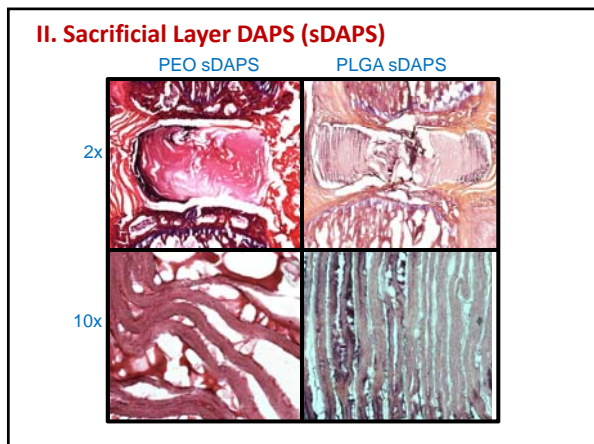
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### Discussion

- Developed an engineered disc that mimics the hierarchical structure of the native AF in a rat tail model.
  - Improvement from ~50% to 100% successful
  - Useful for evaluation of mechanical stimulation and remobilization
- External fixation improves implant retention.
  - Improvement from ~50% to 100% successful
  - Useful for evaluation of mechanical stimulation and remobilization
- Sacrificial layers improve cellular ingress and matrix deposition.
  - Useful in vitro paradigm for construction of cell-seeded DAPS
  - Polymer dissolution time should be tuned for in vivo application

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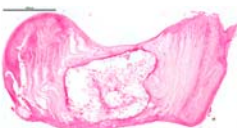
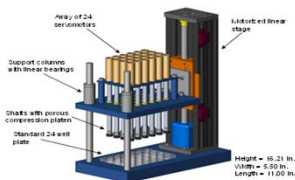
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### Future Directions

- An *in vivo* model to screen:
  - Acellular sDAPS with hydrogel NP
  - Cell-seeded DAPS (comprised of both native NP and AF cells as well as MSCs)
  - Effect of pre-maturation and mechanical stimulation of cell-seeded DAPS and functional outcomes in vivo
  - Methods to improve integration with vertebral endplate
  - Up-scaling to larger species

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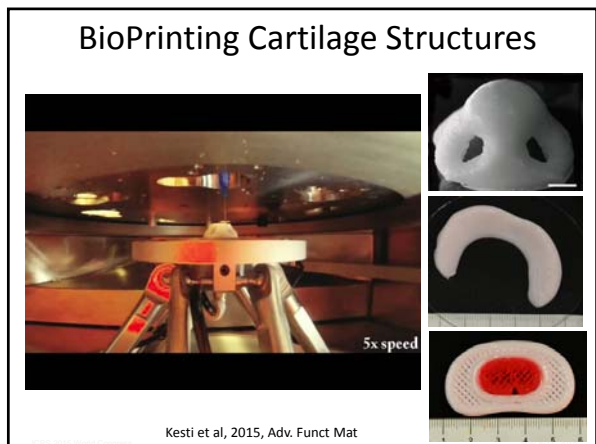
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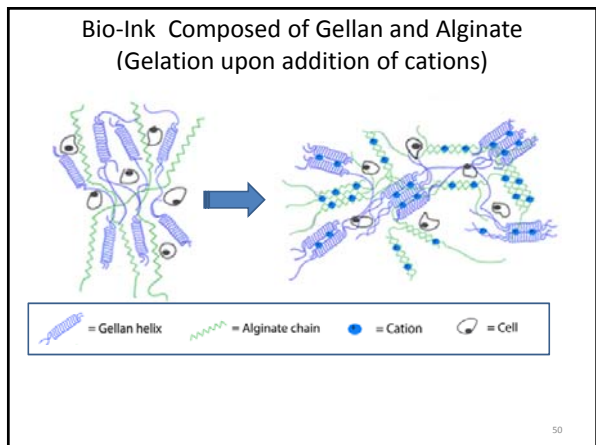
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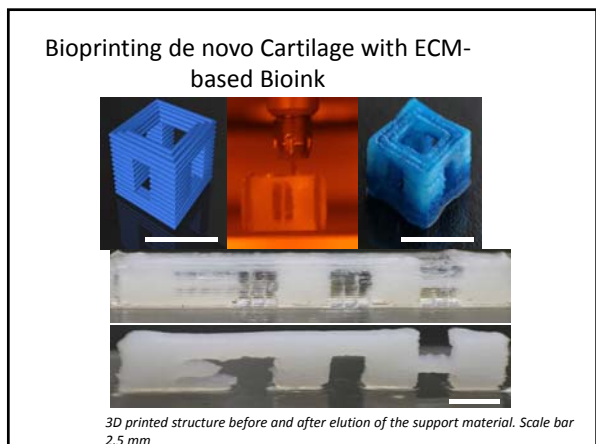
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### 3D Bio printed Components



Multi material samples with varying geometry and structure.




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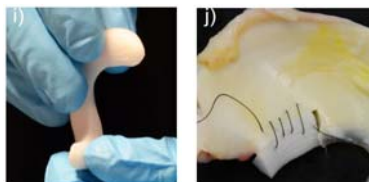
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### How Strong, Flexible, Tough is the Printed Material?



Kesti et al, 2015, Adv. Funct Mat, in press

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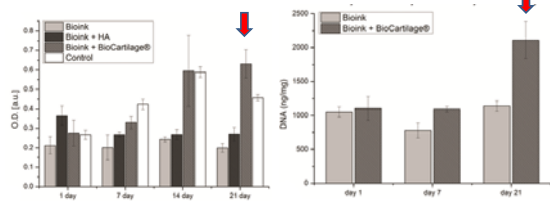
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### Metabolic activity and proliferation increased in the presence of BioCartilage



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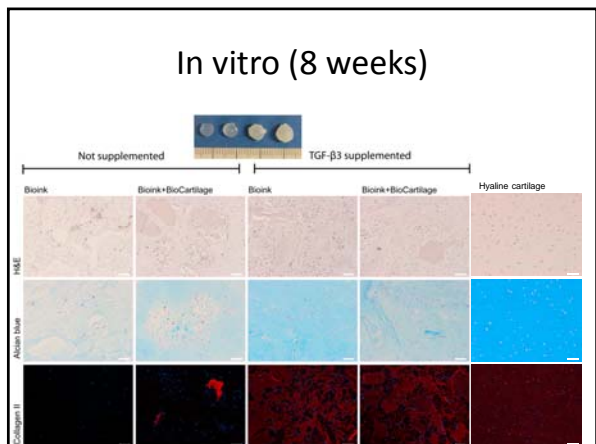
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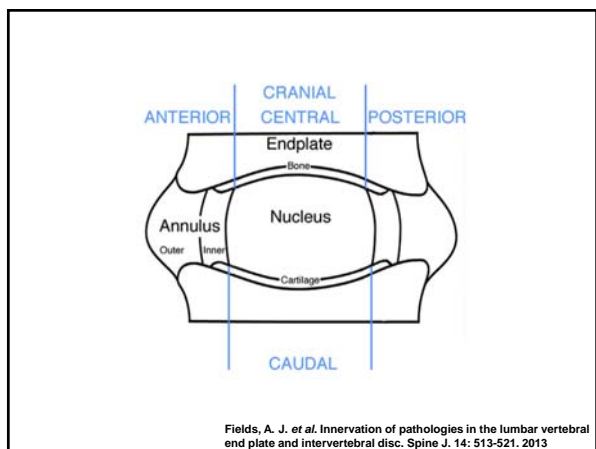
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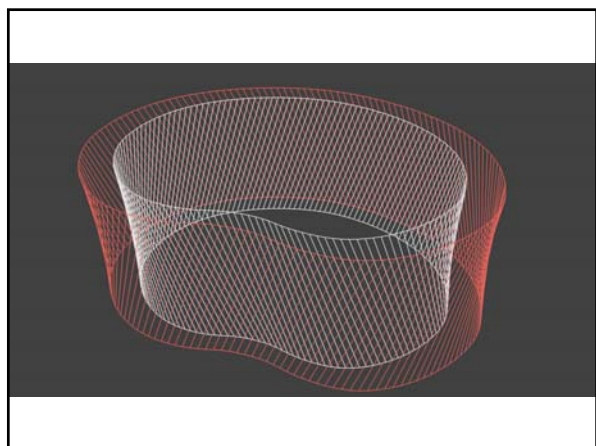
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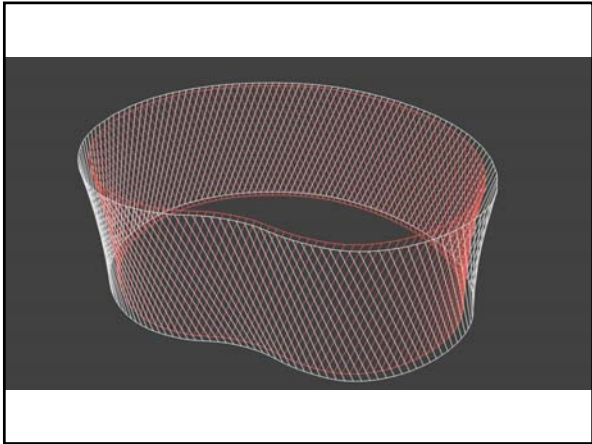
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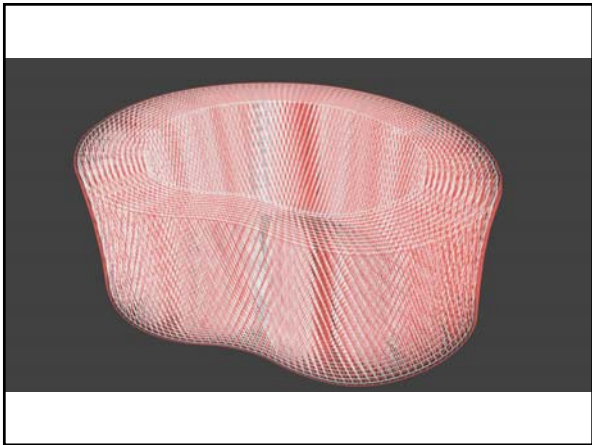
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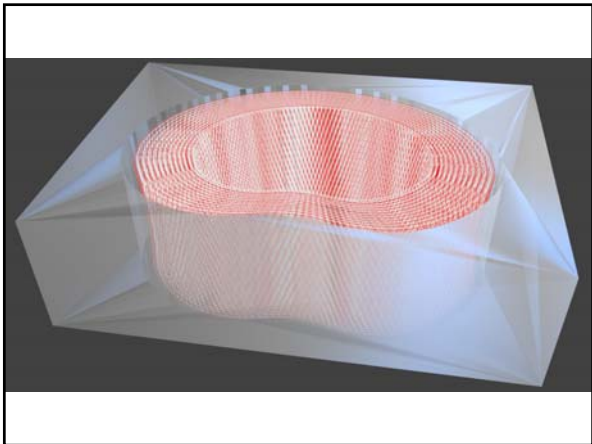
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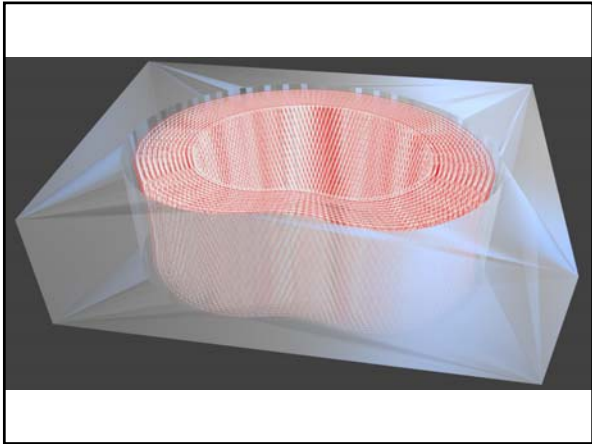
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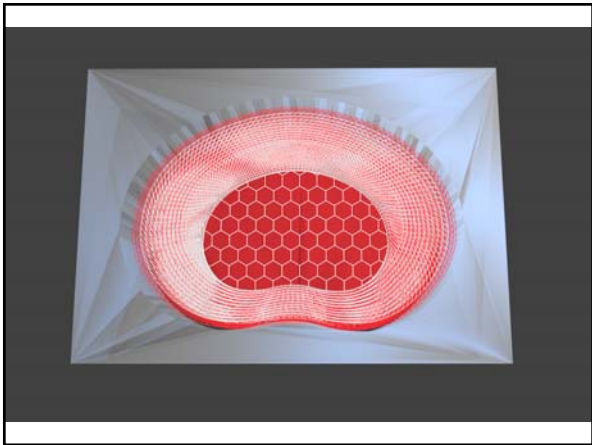
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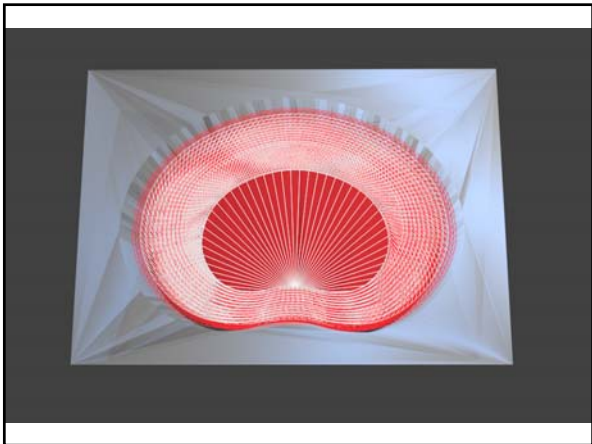
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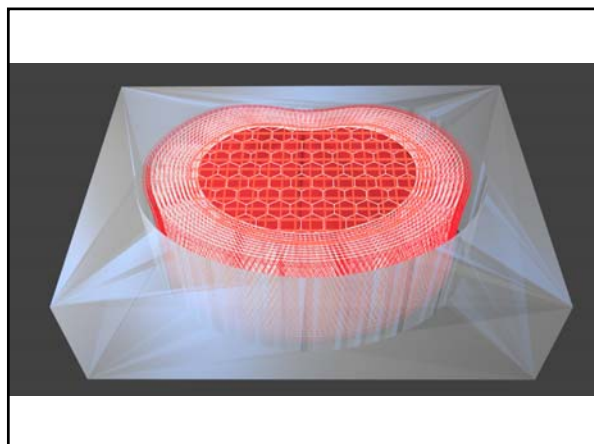
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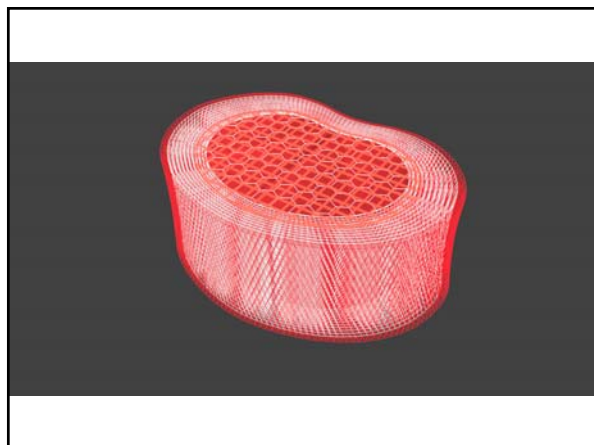
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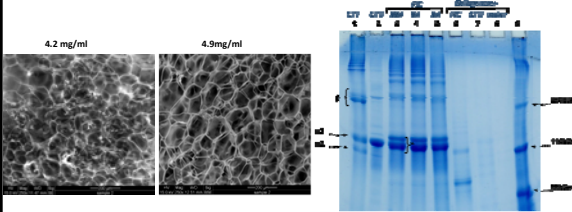
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### Novel Collagen II Scaffold and Gels



The figure shows two scanning electron microscope (SEM) images of scaffolds on the left, labeled '4.2 mg/ml' and '4.9 mg/ml'. To the right is an SDS-PAGE gel with lanes labeled 'C1', 'C2', 'C3', 'C4', 'C5', 'C6', 'C7', 'C8', 'C9', 'C10', 'C11', 'C12', 'C13', 'C14', 'C15', 'C16', 'C17', 'C18', 'C19', 'C20'. Molecular weight markers are indicated on the right at 200kDa, 150kDa, and 100kDa.

*Collagens was extracted from jellyfish umbrella. Pepsinized jellyfish collagens (PIC) were loaded on SDS-PAGE gel (Lane 3-5). Type I (Lane 1) and type II (Lane 2) collagens was used as collagen control. PIC and collagen type II std were treated with collagenase. Molecular mass markers (kDa) are indicated in Lane*

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## Thank You!

- Dept. of Orthopaedic Surgery
- Dept. of Thoracic Surgery
- Dept. of Otolaryngology
- North Shore-LIJ Health System
- Hofstra North Shore-LIJ School of Medicine




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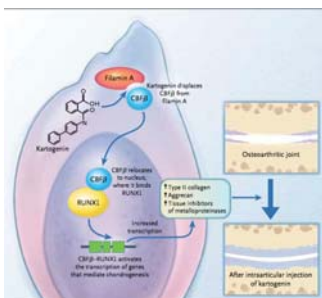
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## Kartogenin Pathway

- Kartogenin binds with filamin A, which normally sits bound with core-binding factor  $\beta$  (CBF $\beta$ )
- Kartogenin displaces CBF $\beta$ , where it migrates to the nucleus and binds with RUNX-1 (transcription factor)
- CBF $\beta$ -RUNX-1 complex increases the transcription of type II collagen, aggrecan, and metalloproteinase inhibitors
- Encourage differentiation into chondrocytes




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## MSC-Derived EVs:

- Stimulate cartilage regeneration
- Enhance proliferation
- Possess anti-inflammatory properties
  
- Clinically safer - no DNA carried
- Cheaper in production and storage
- Easier to biologically manipulate
  
- Regenerative and anti-inflammatory properties →  
→ Potential therapy for OA

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